Glaucoma

Intraday Repeatability of Bruch’s Membrane Opening-Based Neuroretinal Rim Measurements

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PURPOSE. To assess possible intraday variability in Bruch’s membrane opening–based (BMO) assessment of neuroretinal rim by spectral-domain optical coherence tomography (SD-OCT) of the optic nerve head (ONH) as well as its independence from intradividual IOP changes.

METHODS. In this noninterventional, prospective cohort study, 51 consecutively enrolled patients with glaucoma or ocular hypertension underwent standardized SD-OCT of the ONH and IOP assessment at two different time points with a time gap of 5 hours on the same day. Random effects models, intraclass correlation coefficients (ICC) and Bland-Altman plots were used to analyze repeatability of BMO minimum rim width (BMO-MRW) and area (BMO-MRA) and peripapillary retinal nerve fiber layer (RNFL) thickness measurements.

RESULTS. Mean BMO area was 1.86 ± 0.30 mm². At baseline, mean BMO-MRW was 206.46 ± 0.86 µm, mean BMO-MRA was 0.89 ± 0.54 mm², and mean RNFL thickness was 71.61 ± 0.20 µm. Within intradividual measurements, mean difference was 2.95 µm or 1.76% for BMO-MRW, 0.02 mm² or 2.68% for BMO-MRA, and 1.18 µm or 1.89% for RNFL thickness. Comparing time points, \( \eta^2 \) was 0.001 (\( P = 0.757 \)) for RNFL thickness, 0.043 (\( P = 0.01 \)) for BMO-MRA, and 0.07 (\( P = 0.06 \)) for BMO-MRW. Intraclass correlation coefficients were greater than 0.994, respectively. Variability of morphometric parameters did not correlate to intradividual IOP fluctuations.

CONCLUSIONS. Assessment of BMO-MRW by SD-OCT shows high intraday repeatability, which is comparable to the parameter RNFL thickness. Variability seems not to be driven by typical moderate intraday fluctuations of IOP. The two-dimensional parameter BMO-MRA incorporates a fairly higher intradividual variability.

Keywords: Bruch’s membrane opening-based neuroretinal rim measurements, inter-measurement variation analysis, SD-OCT of the optic nerve head

Spectral-domain optical coherence tomography (SD-OCT) of the optic nerve head (ONH) becomes more and more the current gold standard for morphometric assessment in glaucoma diagnostics and follow-up. This technique excels previous approaches as confocal scanning laser tomography by a superior diagnostic power to detect glaucoma and relative observer independency. Retinal structures between Bruch’s membrane opening (BMO) and the internal limiting membrane (ILM) are assessed. Additionally, subsurface structures are analyzed. Correlation of morphometric parameters of the ONH and visual field function has been evaluated in several studies. In addition to the clinically available parameters Bruch’s membrane opening–based minimal rim width (BMO-MRW) and peripapillary retinal nerve fiber layer (RNFL) thickness, two studies on the two dimensional parameter Bruch’s membrane opening minimal rim area (BMO-MRA) showed high diagnostic power for all ONH sizes and equalized differences in BMO-MRW between very large and very small ONHs.

As follow-up data become available, first studies were conducted to assess the performance of SD-OCT for detection of progression of glaucomatous damage to the ONH. Those studies have shown a relative superiority for the parameter RNFL thickness over rim-based parameters. One hypothesis for this finding was the presence of intraday fluctuations of anatomic ONH structures due to vascular and intraocular as intrathecal pressure changes. While some studies focused on the consistency of BMO detection, it was unclear whether intraday changes in parameters depending on the examination time were present.

In the present study, we prospectively recruited a cohort of 51 patients with glaucoma or suspicion of glaucoma, which were hospitalized for 24-hour IOP measurements to compare two SD-OCT examinations of the ONH with a time difference of 5 hours.

METHODS

Data for this single-center, prospective study were acquired from October to December 2016 at the Department of Ophthalmology, University Hospital of Cologne, Germany. Patients received SD-OCT measurements of the ONH at two different time points on the same day. The first examination was conducted during the late morning between 11:00 AM and 12:00 PM, while the second examination took place around 5
In several participants, an additional third SD-OCT measurement had been acquired during clinical routine 24 hours before the first study assessment. Intraocular pressure was measured by corneal rebound tonometry directly before every SD-OCT examination was initiated (Icare tonometer TA01; Icare Finland Oy, Vantaa, Finland).55,27

**Inclusion and Exclusion Criteria**

Inclusion criteria were hospitalization for 24-hour IOP measurement due to presence of glaucoma or suspicion of glaucoma in clinical assessment. Written informed consent was obtained from all participants. Only examinations with an image quality index of greater than 15 dB were included in the analysis. Exclusion criteria were insufficient of clear optical media defined by the ability to reach a sufficient SD-OCT quality index as defined, retinal, or other pathology presenting any potential bias for imaging analysis (e.g., ONH drusen, peripapillary choroidal neovascularization, significant epiretinal membrane), inability for accurate fixation, recent intraocular surgery (<7 days), or other causes for hospitalization that defined within the inclusion criteria.

Participants’ eyes were classified into three groups according to their peripapillary global RNFL thickness to reflect the degree of damage in neuroretinal tissue. Normal global RNFL was defined as thickness of larger than 85 μm. Moderate damage was defined as thinning of RNFL to 65 to 84 μm, while severe damage was indicated by a global RNFL thickness of less than 64 μm.

**Morphometric Analyses of the Optic Disc**

Spectral-domain OCT examinations were performed by Spectralis SD-OCT (Heidelberg Engineering GmbH, Heidelberg, Germany) according to standard operating and imaging procedures using a light source of 870 nm. Included OCT data comprised an image quality index of greater than 15 dB. The scanning pattern was centered on the BMO with radial equidistance (24-high resolution 15° radial scans, each averaged from 27 B-scans). The examiners controlled the centration of the scan to the optic disc and corrected errors in detection of ILM and BMO. Two reviewers assessed independently especially those cases with discrepancies between measurements to exclude bias by manual correction. Optical coherence tomography-based parameters BMO-MRW and BMO area as well as RNFL thickness were calculated by the device operating software tool provided by Heidelberg Engineering, including a data export batch provided by the manufacturer. Bruch’s membrane opening MRA calculation was performed by Heidelberg Engineering software Spectralis SP-X VWM. Gardiner and associates1 proposed the principle of BMO-MRA calculation.

**Electrics and Statistics**

Formal approval to conduct this study was obtained from the Ethics Committee of the University of Cologne (No. 16-340). Written informed consent has been obtained of all participants prior to additional SD-OCT and IOP assessments. All tenets of the Declaration of Helsinki have been regarded. Statistical analyses were performed by SPSS (version 22.0; IBM Corp. Armonk, NY, USA). Differences between time points and differences between absolute relative changes of MRW, MRA, and RNFL were examined using random effects models. Type A intraclass correlation coefficients (ICC) as well as Bland-Altman plots were used. Spearman’s rank correlation analysis was used to test for correlation between morphometric parameters and.

### Table 1. Baseline Data and Optic Nerve Head Morphometrics

<table>
<thead>
<tr>
<th>Time of Examination</th>
<th>First Examination</th>
<th>Second Examination</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mean ± SD</td>
<td>11.32 ± 0.23</td>
<td>16.52 ± 0.26</td>
</tr>
<tr>
<td>Sex, n (%)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Men</td>
<td>45 (46.4)</td>
<td>-</td>
</tr>
<tr>
<td>Women</td>
<td>52 (53.6)</td>
<td>-</td>
</tr>
<tr>
<td>Age, y</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>63.6 ± 15.5</td>
<td>-</td>
</tr>
<tr>
<td>Median</td>
<td>67.2</td>
<td>-</td>
</tr>
<tr>
<td>Eye, n (%)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Right</td>
<td>48 (49.5)</td>
<td>-</td>
</tr>
<tr>
<td>Left</td>
<td>49 (50.5)</td>
<td>-</td>
</tr>
<tr>
<td>Lens status (%)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Phakic</td>
<td>62</td>
<td></td>
</tr>
<tr>
<td>Pseudophakic</td>
<td>35</td>
<td></td>
</tr>
<tr>
<td>Uncorrected refractive error, n = 69, D</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Spherical equivalent (SE)</td>
<td>0.05 ± 2.94</td>
<td></td>
</tr>
<tr>
<td>Range</td>
<td>-8.00 to +6.4</td>
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</tr>
<tr>
<td>Number of patients</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>exceeding SE of ±5.0 D (n)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Current refractive error (scan focus, D)</td>
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<td></td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>-0.80 ± 1.36</td>
<td>-</td>
</tr>
<tr>
<td>IOP mm Hg</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>14.5 ± 4.8</td>
<td>13.8 ± 3.7</td>
</tr>
<tr>
<td>Mean global BMO area, mm²</td>
<td>1.86 ± 0.30</td>
<td>1.86 ± 0.31</td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>206.46 ± 85.88</td>
<td>205.24 ± 85.71</td>
</tr>
<tr>
<td>Mean global BMO-MRA, μm</td>
<td>0.89 ± 0.03</td>
<td>0.88 ± 0.03</td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>71.61 ± 19.64</td>
<td>71.56 ± 19.45</td>
</tr>
</tbody>
</table>

IOP: The threshold for statistical significance was *P* less than 0.05

**Results**

In this prospective study, 51 patients were enrolled, whereof 97 eyes could be included in the analyses. In five eyes of these patients, insufficient image quality (four eyes) or data acquisition errors (one eye) led to exclusion. Epidemiology and baseline data are summarized in Table 1.

In all included eyes, mean BMO area was 1.86 ± 0.30 mm². The first SD-OCT examination was conducted in average at 11:32 AM (range, 10:58 AM to 12:45 PM), the second examination at 4:54 PM (range, 4 to 5:50 PM) resulting in a mean interval of 5.4 hours. Mean BMO-MRW in the first examination was 206.46 ± 0.86 μm (range, 50.26–508.38 μm), mean BMO-MRA was 0.89 ± 0.34 mm² (range, 0.28–1.94 mm²), and mean RNFL thickness was 71.61 ± 0.20 μm (range, 34–111 μm).

At the second SD-OCT examination, mean BMO-MRW was 205.24 ± 0.86 μm (range, 54.78–501.03 μm), mean BMO-MRA...
was 0.88 ± 0.34 mm² (range, 0.30–1.88 mm²), and mean RNFL thickness was 71.56 ± 0.19 µm (range, 34–111 µm).

Repeatability Analyses of Morphometric Intraday Measurements

Mean difference between absolute intraindividual measurements was 2.95 µm or 1.76% for BMO-MRW, 0.02 mm² or 2.68% for BMO-MRA, and 1.18 µm or 1.89% for RNFL thickness. While BMO-MRW and RNFL thickness demonstrated a comparable relative change between intraday measurements ($P = 0.45$), BMO-MRA showed significantly higher intraindividual variability compared with BMO-MRW ($P < 0.001$) and RNFL thickness ($P = 0.008$). Comparison of time points resulted in $\eta^2 = 0.001$ with $P = 0.757$ for RNFL thickness, $\eta^2 = 0.04$ with $P = 0.06$ for BMO-MRW, and $\eta^2 = 0.07$ with $P = 0.01$ for BMO-MRA.

Figures 1 through 3 show Bland-Altman plots for graphical display of intraday repeatability of the three morphometric measurements.

**Figure 1.** Bland-Altman plot for intraday repeatability of BMO-MRW measurements.

**Figure 2.** Bland-Altman plot for intraday repeatability of RNFL thickness measurements.
parameters. Intraclass correlation coefficients 95% confidence intervals (CI) were 0.994 to 0.997 for RNFL thickness ($P < 0.001$), 0.999 to 1.0 for BMO-MRW ($P < 0.001$), and 0.994 to 0.998 for BMO-MRA ($P < 0.001$).

Reproducibility of SD-OCT Segmentation and Intraday IOP Measurements

In 55 of 97 eyes, ILM and BMO detection was highly reproducible. In those eyes, manual correction of ILM or BMO was necessary in only less than three of 24 scans. In this group, mean differences between absolute intraindividual measurements of all the parameters were not different from those of the entire cohort. Regarding BMO correction solely, 80.4% of all eyes included in this study had equal or less than 8 scans with BMO corrections in two examinations, resulting in less than four corrections per examination. Additionally, results for parameters BMO area and BMO-MRW were compared with and without manually correction. In all eyes included, mean corrected BMO area was $1.865 \pm 0.30 \text{ mm}^2$ in the morning and $1.861 \pm 0.31 \text{ mm}^2$ in the evening resulting in a difference of $0.004 \text{ mm}^2$. Mean uncorrected BMO area was $1.839 \pm 0.31 \text{ mm}^2$ and $1.830 \pm 0.32 \text{ mm}^2$ respectively, resulting in a difference of $0.009 \text{ mm}^2$.

Mean IOP was $14.49 \text{ mm Hg}$ (range, $7–31 \text{ mm Hg}$) at the first and $13.77 \text{ mm Hg}$ (range, $7–22 \text{ mm Hg}$) at the second examination. Intraindividual absolute mean change of IOP between the two measurements was $2.7 \text{ mm Hg}$. Intraindividual variability in morphometric parameters did not correlate significantly with intraindividual changes of IOP ($\rho = 0.1–0.2; P > 0.12$).

Repeatability Analysis According to Peripapillary Global RNFL Thickness Subgroups

Global RNFL thickness in the first measurement was larger than $85 \mu\text{m}$ in 29 eyes, between $65$ and $84 \mu\text{m}$ in 32 eyes and less than $64 \mu\text{m}$. Between those groups, relative change between intraday measurements increased toward higher degree of ONH damage, for BMO-MRW from $1.2\%$ to $2.4\%$ ($P = 0.05$), for RNFL thickness from $0.9\%$ to $2.5\%$ ($P < 0.001$), and for BMO-MRA from $2.4\%$ to $3.0\%$ ($P = 0.59$).

Supplemental Examination With a 24-Hour Time Gap

In 48 eyes, a third SD-OCT examination was conducted within clinical routine diagnostics for glaucoma evaluation with a...
Intraday Repeatability in SD-OCT for Glaucoma

mean interval of 22.9 hours before or after the first study examination in average at 11:54 AM in the morning hours.

Mean BMO-MRW in this supplemental examination was $216.46 \pm 0.35 \, \mu m$ (range, 52.25–404.05 \, \mu m), mean BMO-MRA was $0.91 \pm 0.35 \, mm^2$ (range, 0.28–1.65 \, mm^2), and mean RNFL thickness was $74.74 \pm 0.20 \, \mu m$ (range, 36–102 \, \mu m).

For intraindividual measurements, mean difference of absolute values between the supplemental examination and the first examination of the study was $3.74 \, \mu m$ or 2.14% for BMO-MRW, 0.03 mm^2 or 3.19% for BMO-MRA, and 2.07 \, \mu m or 3.22% for RNFL thickness. Proportional frequency in relative change between measurements was lower for BMO-MRW compared with BMO-MRA ($P = 0.008$) and to RNFL thickness ($P = 0.12$).

Results of random effects models with repeated measures did not reach the defined level for statistical significance.

**Discussion**

Morphometric assessment of the ONH by SD-OCT has become a cornerstone in glaucoma diagnostics and follow-up. Diagnostic power to detect and differentiate glaucomatous damage in a single observation has been analyzed in numerous studies for a broad range of clinical and anatomic situations.

As follow-up data after introduction of this technique become more and more available, first results seem to demonstrate a superior correlation of peripapillary RNFL thickness to functional loss in visual field testing compared with BMO-based parameters. A possible explanation of this inferiority of BMO-based parameters to detect change was thought in a higher variability of measurements due to fluctuations in anatomic ONH structures. Consistency of BMO detection of the ONH in Cirrus SD-OCT was evaluated by Hwang and associates, who found overall satisfactory consistency levels and higher discrepancies in myopic eyes with peripapillary atrophy. In another study of Pearce et al., intervisit test-retest variability of OCT in glaucoma was excellent for horizontal and vertical cup/disc ratios and ganglion cell complex. Mansouri et al. reported good correlations between OCT measurements in sitting and supine positions and high repeatability of measurements of ONH and RNFL.

In this study, we could show that BMO-MRW and RNFL thickness parameters show a high degree of consistency between measurements in the morning and in the afternoon. Relative change of absolute differences between examinations in these two standard parameters does not show a statistically significant difference, ICC, and Bland-Altman plots support this conclusion. BMO-based minimum rim area (BMO-MRA) has been proposed as an additional, three-dimensional parameter to measure the neuroretinal rim by SD-OCT. Bruch’s membrane opening MRA has been shown to offer higher comparability between differences in ONH sizes. Bruch’s membrane opening MRA showed a significantly higher relative intraindividual variability between both examinations on the same day. As BMO area measurements were stable, reason for this might be the more complex calculation algorithm of this two-dimensional parameter with independent localized minimization of 48 trapezoids.

Toward progressive damage of neuroretinal tissues, we did find a slight but significant increase in variability between intraday measurements. This increase was statistically significant for BMO-MRW and RNFL thickness parameters. A reason for this might be the device-specific variation, which is constant for all measurements but gains relative relevance when morphometric parameters worsen. Changes in IOP could represent an additional factor influencing ONH morphology analyzed by SD-OCT. In our study, intraday IOP fluctuations were moderate between both measurements. The effects of higher changes in IOP on morphology, for example, before and after trabeculectomy, remain unclear and should be focus on an additional study.

Incorrect automated detection of ILM or BMO structures by the operating software requiring consecutive manual correction might represent another reason for intraindividual variation between two measurements. In our study, manual correction of Bruch’s membrane ending had an effect on the BMO area size but seemed not to have affected the parameter BMO-MRW. It is not surprising that BMO area size is affected by manual correction, as the calculation algorithms tend to face difficulties in detection of Bruch’s membrane ending when border tissue of Elschnig is present in peripapillary atrophy. In consequence, true BMO area is larger than measured by the automated algorithm. Intraday variability between the two measurements was at the same level regardless of whether BMO correction was applied or not.

Variation in vascular components of the analyzed anatomic structured might also be responsible for intraindividual variation in measurements. That question was not in scope of our study. Future studies assessing vascular parameters (e.g., blood pressure, choroidal thickness, vascular density in Angio-OCT) need to be undertaken.

Limitations to the study are the missing information on the original refractive status prior to cataract surgery in 30% of the patients and the absence of axial length measurements in all eyes. For future studies, obtaining this information in all patients would be desirable.

To summarize the main conclusions of the present study, we did not find any relevant intraday variability in SD-OCT based morphometric parameters between measurements taken with a time gap of 5 hours. Intrascan correlation coefficients levels were excellent. Variations in diagnostic power to detect progression between BMO-based parameters and peripapillary rim measurements seem not to be driven by intraday fluctuations of ONH morphology or by changes in IOP.

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**References**


